

SPECTRAL ANALYSIS

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- (Example of coherence function)

Fourier-based power spectrum analysis

• The estimated power spectrum (periodogram) of a stationary signal x[n] (x[n] is assumed to be zero outside the interval [0, N - 1]), is obtained by computing the squared magnitude of the N-point DTFT of x[n]

$$\widehat{S}_{x}(\omega) = \frac{1}{N} \left| X(\omega) \right|^{2} = \frac{1}{N} \left| \sum_{n=0}^{N-1} x[n] e^{-j\omega n} \right|^{2}$$

 Since N-point DFT completely specifies the DTFT of a finite duration sequence of length N samples, the estimated power spectrum (periodogram) of a stationary signal x[n] can simply be computed following

$$P[k] = \frac{1}{N} |X(k)|^{2} = \frac{1}{N} \left| \sum_{n=0}^{N-1} x[n] e^{j(\frac{2\pi k}{N})n} \right|^{2}$$

• Parseval's theorem expresses the energy in the finite duration sequence x[n] in terms of the frequency components X[k]

$$\sum_{n=0}^{N-1} x[n]^2 = \frac{1}{N} \sum_{k=0}^{N-1} |X[k]|^2$$

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Joint time-frequency analysis

- A major limitation of Fourier-based spectral analysis is its inability to provide information on when in time different frequencies of a signal occur
- The Fourier transform only reflects which frequencies exist during the total observation interval, because the Fourier transform integrates frequency components over the total observation interval
- While such spectral analysis is adequate for stationary signals whose frequencies, on average, are equally spread in time, it is inadequate for nonstationary signals with time dependent spectral content
- There is strong motivation for the development of methods that analyze signals with regard to both time and frequency so that the frequencies present at each instant in time can be displayed
- Joint time-frequency information has been found extremely valuable for many types of biomedical signals exhibiting non-stationary characteristics



The short-time Fourier transform

• The short-time Fourier transform is a classical non-parametric method to obtain time-frequency representation by linear filtering operation



• In the short-time Fourier transform, a sliding time window $w(t - \tau)$ is used for excerpting successive parts of the signal x(t)

The short-time Fourier transform

• In this approach, the definition of the Fourier transform is modified so that a sliding time window w(t) is included that defines each time segment to be analyzed, thus resulting in a two-dimensional function $X(t, \Omega)$ defined by:

$$X(t,\Omega) = \int_{-\infty}^{\infty} x(\tau) w(\tau-t) e^{-j\Omega \tau} d\tau$$

where Ω denotes analog frequency

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(Sornmo, Laguna) Biomedical signal and image processing $S_w(n_1,m)$

The short-time Fourier transform

 \implies $S(n_1, \omega)$

FT

- Divide a signal into short segments
- Calculate amplitude spectrum for each segment
- Compose time series of spectra
- Short-time Fourier transform of word "devet"

Spectrogram

 Analogous to the computation of the periodogram, which was obtained as the squared magnitude of the Fourier transform of the signal:

$$\widehat{S}_{x}(\omega) = \frac{1}{N} \left| X(\omega) \right|^{2} = \frac{1}{N} \left| \sum_{n=0}^{N-1} x[n] e^{-j\omega n} \right|^{2}$$

the spectrogram, $S_x(t, \Omega)$, of x(t) is obtained by computing the squared magnitude of the short-time Fourier transform:

$$S_x(t, \Omega) = |X(t, \Omega)|^2$$

where

$$X(t,\Omega) = \int_{-\infty}^{\infty} x(\tau) w(\tau-t) e^{-j\Omega \tau} d\tau$$

• The spectrogram, $S_x(t, \Omega)$, is a real-valued, nonnegative distribution which provides a signal representation in the time-frequency domain

Example

- (a) The EEG recorded during heart surgery of an infant (time scale from 0 to 300 sec)
 - (b) The spectrogram displays a drastic reduction in high-frequency content after 100 s, partially reverting at about 200 s

(Sornmo, Laguna) Biomedical signal and image processing

Amplitude [µV]

Frequency [Hz]

• Rectangular window

• Sinusoid signal, the effect of windowing (rectangular window, length N)

$$x(n) = \cos(\omega_0 n) = \frac{1}{2}e^{-j\omega_0 n} + \frac{1}{2}e^{j\omega_0 n}$$

$$v(n) = x(n)w(n)$$

$$V(e^{j\omega}) = \text{DTFT}[w(n)\left(\frac{1}{2}e^{-j\omega_0 n} + \frac{1}{2}e^{j\omega_0 n}\right)]$$
Since $e^{j\omega_0 n}x(n) \leftrightarrow X(e^{j(\omega-\omega_0)})$

$$V(e^{j\omega}) = \frac{1}{2}W(e^{j(\omega+\omega_0)}) + \frac{1}{2}W(e^{j(\omega-\omega_0)})$$

$$W(e^{j\omega}) = \text{DTFT}[w(n)] = \frac{\sin(\omega N/2)}{\sin(\omega/2)}e^{-j\omega(N-1)/2}$$

$$-\omega_0$$

$$W(e^{j\omega}) = \text{DTFT}[w(n)] = \frac{\sin(\omega N/2)}{\sin(\omega/2)}e^{-j\omega(N-1)/2}$$

[Proakis, Manolakis]

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Biomedical signal and image processing

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• Sinusoid signal, the effect of windowing (rectangular window, length N)

Frequency resolution: $\Delta \omega_R = \frac{2\pi}{N}$ Low resolution $\Delta \omega_R = \frac{2\pi}{N} = \frac{2\pi}{25} = 0.2513 [\frac{rad}{smp}]$ 14 12 10 Frequency resolution: $\Delta f_R = \frac{1}{N}$ Magnitude Leakage $\Delta f_R = \frac{1}{N} = \frac{1}{25} = 0.04 [\frac{cyc}{smp}] => 25 \text{ lobes}$ Frequency resolution: $\Delta F_R = \frac{F_S}{N}$ Frequency $\Delta F_R = \frac{F_S}{N} = \frac{F_S}{25}[Hz]$ \mathcal{W}_0 \mathcal{W}_0

Biomedical signal and image processing

 $\frac{\pi}{2}$

 $V(e^{j\omega})$

N = 25

- The length of the sliding time window *w(t)* determines the resolution in time and frequency such that a short window yields good time resolution but poor frequency resolution, and the opposite when a long window is used
- Rectangular window w(t) causes less reliable measurements on spectral power
- Better estimates of power spectra are obtained by using weighted window functions like Triangular, Hanning, and Hamming windows

Coefficients of window functions

Rectangular window w[n] = 1, n = 0, 1, 2, ..., N-1

Triangular window
$$w[n] = \begin{cases} \frac{n}{N/2}, & n = 0, 1, 2, ..., N/2 \\ 2 - \frac{n}{N/2}, & n = N/2 + 1, N/2 + 2, ..., N - 1 \end{cases}$$

Hanning (Hann) window $w[n] = 0.5 - 0.5 \cos(\frac{2\pi n}{N}), & n = 0, 1, 2, ..., N - 1$
Hamming window $w[n] = 0.54 - 0.46 \cos(\frac{2\pi n}{N}), & n = 0, 1, 2, ..., N - 1 \end{cases}$

• Rectangular window,

Triangular window,

Hanning (Hann) window, Hamming window

Sample 1.0 Rectangular window

(b)

(C)

Time

Sample

[Lyons]

(a)

COULDCE ODDET

• Linear-scale window amplitude spectra, |W(k)|

• Logarithmic-scale window amplitude spectra, |WdB[k]| in dB

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Biomedical signal and image processing

- Sinusoid signal, the effect of windowing
 - Left, amplitude spectrum using rectangular window, N = 25 samples
 - Right, amplitude spectrum using Hanning window, N = 25 samples

Biomedical signal and image processing [Proakis, Manolakis]

Example of spectrogram

- Example of spectrogram using Hamming windows (next slide)
 - (a) The EEG at the onset of an epileptic seizure. The corresponding spectrogram is computed using a Hamming window with a length of(b) 1 s, (c) 2 s, and (d) 0.5 s.
 - (c) The spectrogram is obtained with the longest time window (2 s) and therefore exhibits the poorest time resolution of the three lengths; property is reflected by a ridge which extends longer in time than does the ridge in figure (d)
 - (c) The spectrogram shows the best frequency resolution is due to the longer time window (2 s), while the frequency resolution in figure (d) is worse
- There is always a trade-off with respect to resolution in time and frequency

Example of spectrogram

• Spectrogram of the speech signal (Fs = 16.000 smp/sec; Hamming window, w(n), of duration 6.8 sec, or, N = 108; time increment 16 samples, or 1ms)

(Coherence function)

- The coherence function (magnitude-squared coherence), $C_{xy}(\omega)$, allows us to find common frequencies and to evaluate the similarity of signals
- Coherence (Latin cohaerentia) means natural or logical connection or consistency
- The coherence function estimates the extent to which *y(t)* may be predicted from *x(t)*

$$C_{xy}(\omega) := \frac{P_{xy}(\omega)}{\sqrt{P_{xx}(\omega)P_{yy}(\omega)}} \qquad P_{xx}(\omega) := |\hat{x}(\omega)|^2 = \hat{x}(\omega)\overline{\hat{x}(\omega)}$$
$$P_{xy}(\omega) := \hat{x}(\omega)\overline{\hat{y}(\omega)}$$
$$C_{xy}^2(\omega) = \frac{|P_{xy}(\omega)|}{P_{xx}(\omega)P_{yy}(\omega)} \qquad \hat{x}(\omega) := \int_{-\infty}^{\infty} x(t)e^{-i\omega t}dt$$

where $P_{xx}(\omega)$ and $P_{yy}(\omega)$ are power spectra of signals x(t) and y(t), $P_{xy}(\omega)$ is cross-power spectrum for these signals, and $x^{(\omega)}$ and $y^{(\omega)}$ are the Fourier transforms of x(t) and y(t)

- The value of coherence will always satisfy $0 \le C_{xy}(\omega) \le 1$
- If y[n] = h[n] * x[n], then $C_{xy}(\omega) = 1$

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