# PROCESSING, FEATURE EXTRACTION AND SHAPE REPRESENTATION OF THE ECG, I

- Basic stages of ECG signal processing
- ECG filtering
- Basic stages of ECG signal processing
- QRS complex detection
- The principles of QRS complex detection
- QRS complex detection
- QRS complex detection, performance evaluation
- Heart beat detection in multimodal data
- (Challenges in ECG signal processing today)
- (ECG filtering)
- (ECG filtering, power line interference)
- (Wave delineation)
- (Sophisticated QRS complex detection)
- (QRS complex detection, performance evaluation)

# Basic stages of ECG signal processing

#### • ECG filtering

- QRS complex detection
  - → (Wave delineation)
- QRS complex classification
  - → (Rhythm classification)
  - → Ischaemia detection (classifying ischaemic events, detecting transient ischaemic episodes, and their precise beginnings, extrema and ends)

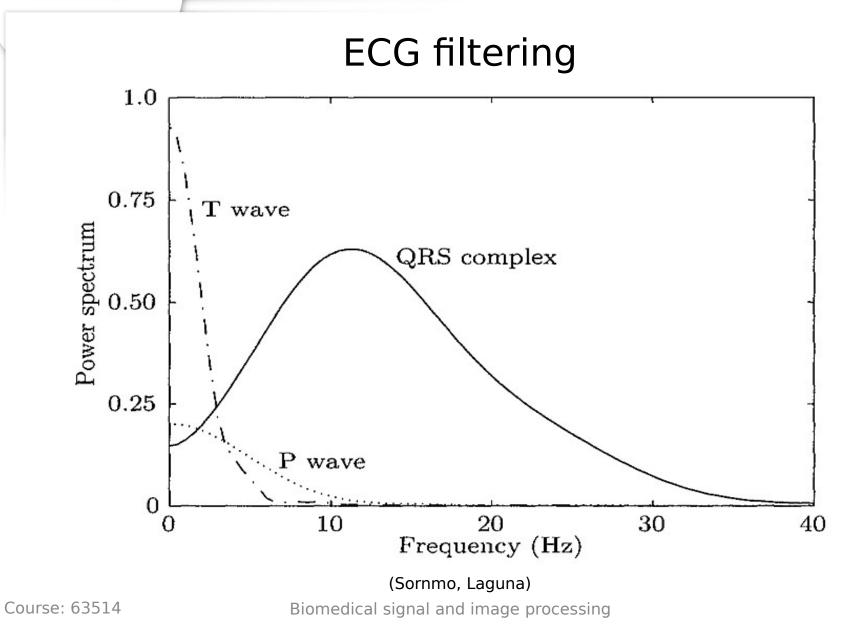


• (a) Baseline wander, (b) electrode motion artifacts, (c) electromyogram noise



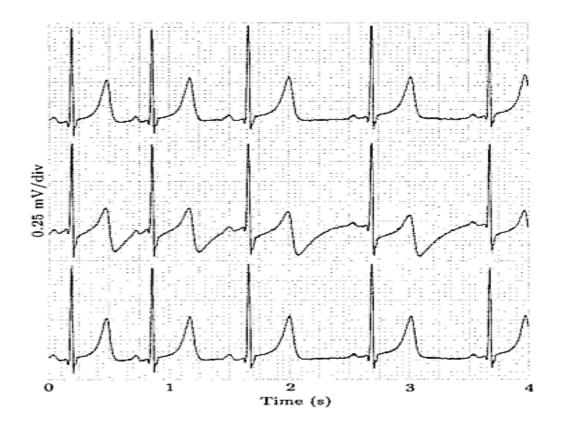
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#### • Linear time-invariant filtering (middle $\rightarrow$ IIR filter, bottom $\rightarrow$ FIR filter)

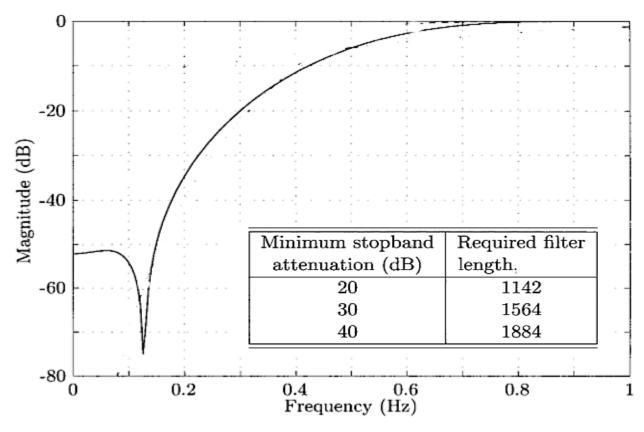


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• FIR filter (1142 coefficients), linear time-invariant filtering (cutoff at *Fc* = 0.6 *Hz*, - 20 dB at 0.3 *Hz*, *Fs* = 250 *smp/sec*)



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6



• The original ECG signal, linear FIR filtering

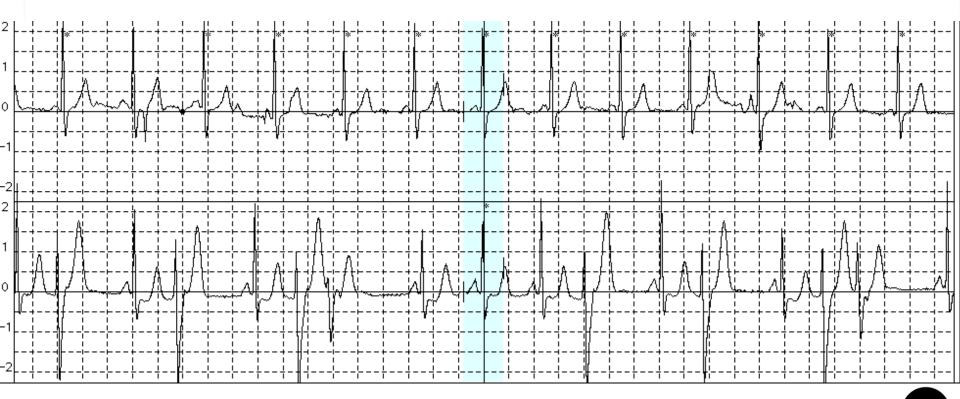


# Basic stages of ECG signal processing

- ECG filtering
- QRS complex detection
  - → (Wave delineation)
- QRS complex classification
  - $\rightarrow$  (Rhythm classification)
  - → Ischaemia detection (classifying ischaemic events, detecting transient ischaemic episodes, and their precise beginnings, extrema and ends)



- Exercises 1.a 1.e: QRS complex detection (detecting heart beats)
- Each heartbeat has QRS complex (a region within heartbeat with highest dynamic)

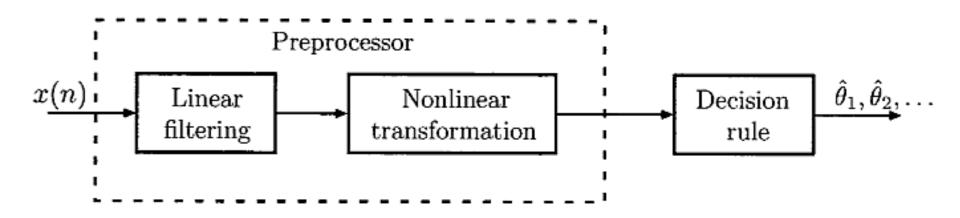


# The principles of QRS complex detection

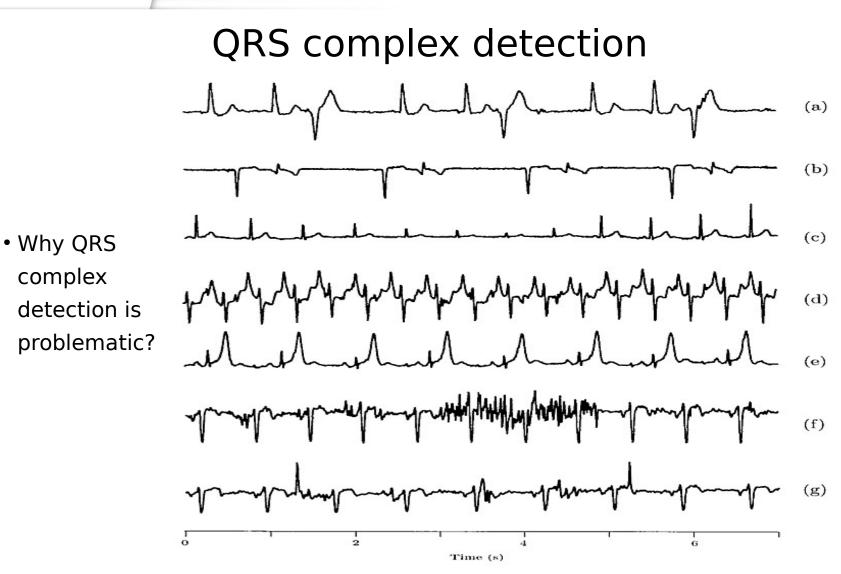
- Approaches based on signal derivatives or digital filters
- Wavelet-based QRS detection approaches
- Approaches based on matched filters
- Other approaches (adaptive filters, hidden Markov models, mathematical morphology, length transform, neural networks, ...)



 Block diagram of a QRS complex detector based on signal derivatives or digital filters





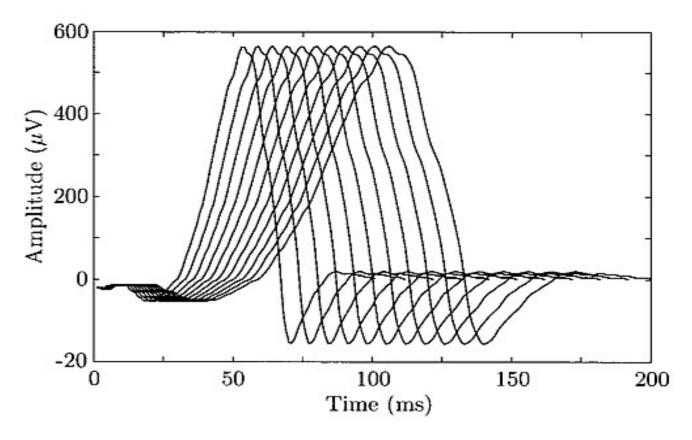


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12



• Why QRS complex detection is problematic? (identical morphology but different durations)

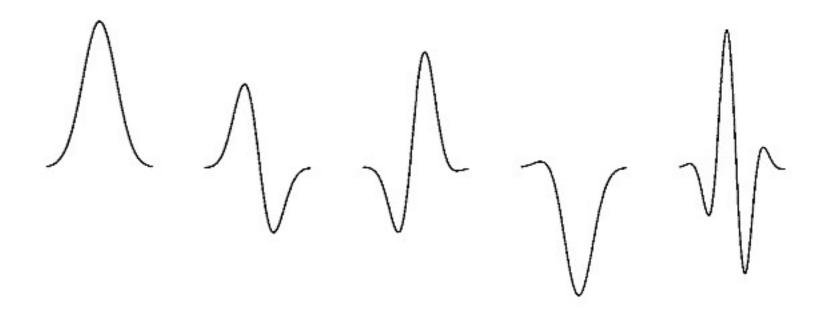


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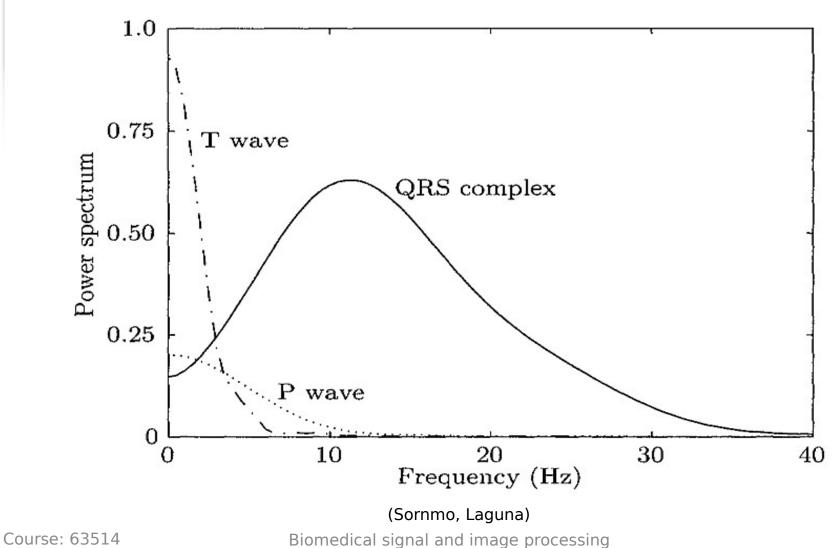


• Why QRS complex detection is problematic? (monophasic and biphasic waveshapes)



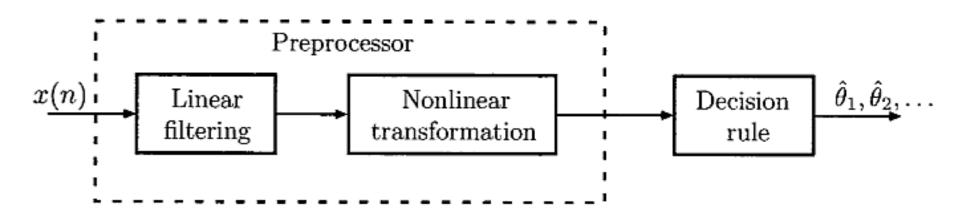
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- Phases of QRS complex detection
  - Linear filtering (extracting/emphasizing slopes and peaks of QRS complex)
  - Nonlinear transformation (energy collector) to get the detection function
  - Decision rule
  - Determining stable fiducial point (FP)





- Linear filtering and nonlinear transformation
  - d[n] detection function
  - N number of simultaneous ECG leads
  - H1 filter sensitive on slopes (Q-R and R-S) of QRS complex
  - H2 filter sensitive on peaks (Q, R, and S) of QRS complex
  - G low-pass moving average filter

$$d[n] = G\left(\left(\sum_{i=1}^{N} \left(|H_{1}(x_{i}[n])| + |H_{2}(x_{i}[n])||\right)|^{2}\right)\right)$$



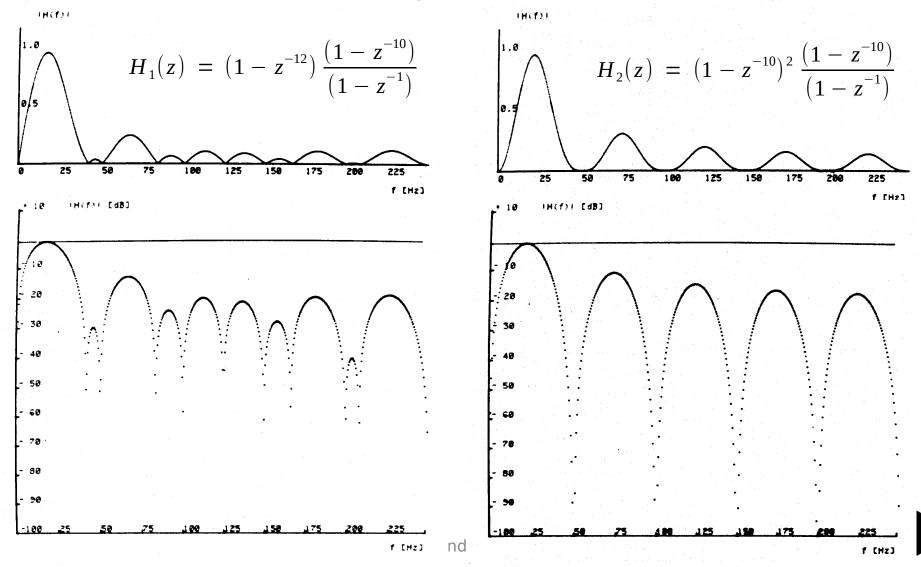
• Linear filtering

 $(H_1(z) - \text{extracts slopes}, H_2(z) - \text{extracts peaks}, F_s = 500 \text{ smp/sec})$ 

$$d[n] = G\left(\left(\sum_{i=1}^{N} \left(|H_{1}(x_{i}[n])| + |H_{2}(x_{i}[n])||\right)|\right)^{2}\right)$$
$$H_{1,2}(z) = (1 - z^{-m})^{M} \frac{(1 - z^{-n})}{(1 - z^{-1})}$$
(1)

$$H_1(z) = (1 - z^{-12}) \frac{(1 - z^{-10})}{(1 - z^{-1})} \quad H_2(z) = (1 - z^{-10})^2 \frac{(1 - z^{-10})}{(1 - z^{-1})}$$

#### QRS complex detection



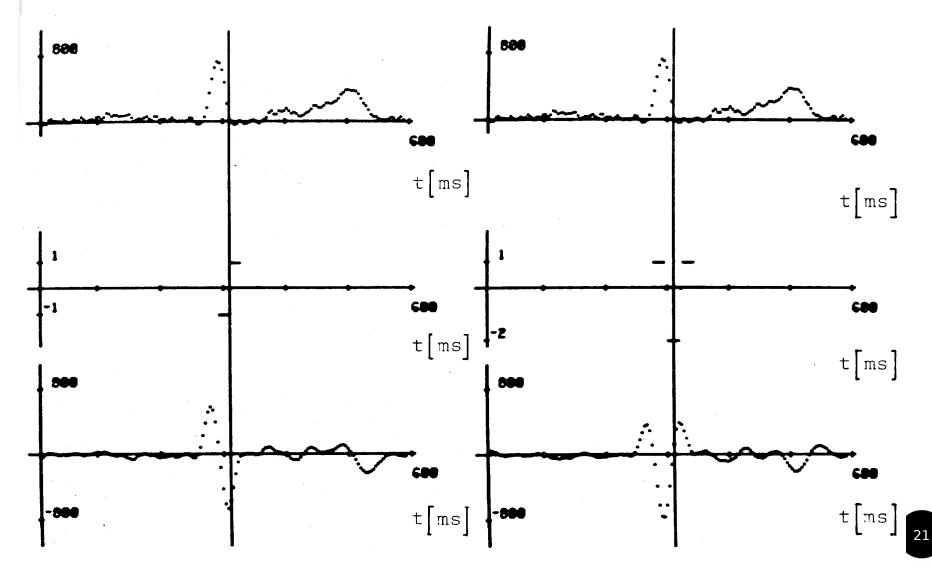
• Linear filtering

 $H_1(z) = (1 - z^{-12}) \frac{(1 - z^{-10})}{(1 - z^{-1})}$ 

- Transfer functions
- Difference equations
- Impulse responses

$$H_2(z) = (1 - z^{-10})^2 \frac{(1 - z^{-10})}{(1 - z^{-1})}$$

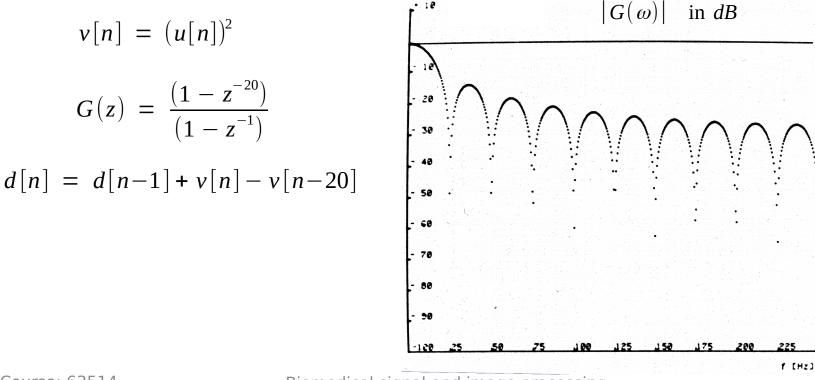
$$y_{1,i}[n] = y_{1,i}[n-1] + x_i[n] - x_i[n-10] - x_i[n-12] + x_i[n-22]$$
  
$$y_{2,i}[n] = y_{2,i}[n-1] + x_i[n] - 3x_i[n-10] + 3x_i[n-20] - x_i[n-30]$$





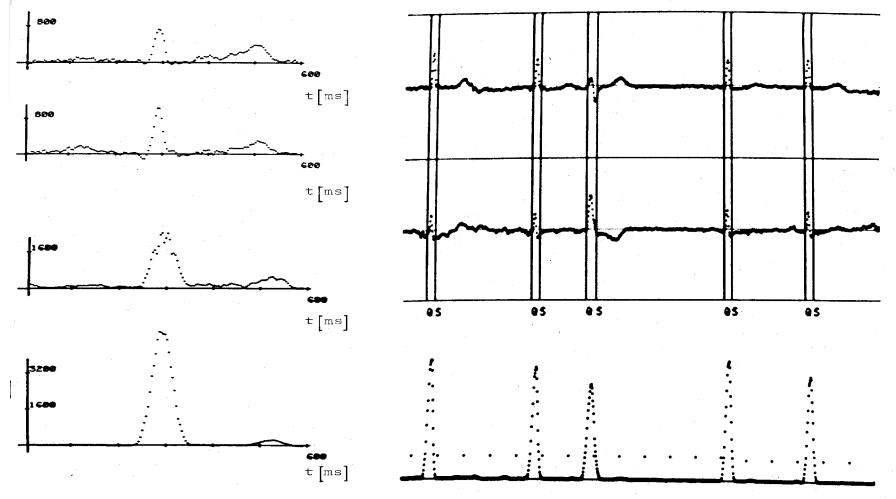
 Nonlinear transformation

$$d[n] = G\left(\left(\sum_{i=1}^{N} \left(|H_{1}(x_{i}[n])| + |H_{2}(x_{i}[n])||\right)|^{2}\right)\right)$$
$$u[n] = \sum_{i=1}^{N} \left(|y_{1,i}[n - (T_{2} - T_{1})]| + |y_{2,i}[n]|\right)$$



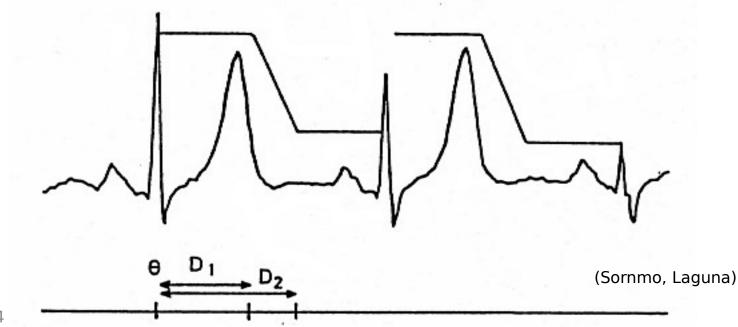


• Original signals, after filtering and summing, and the detection function, d[n]



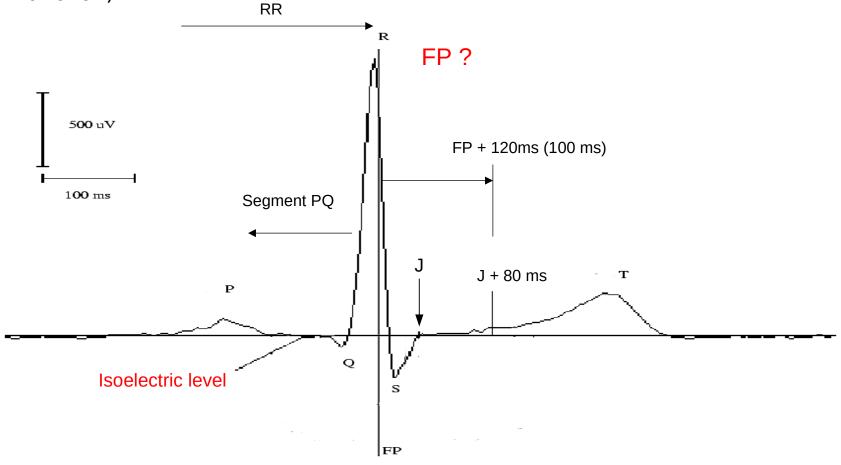


• Decision rule  $\eta[n] = \begin{cases} \alpha_1, & n = \theta + 1, \dots, \theta + D_1 \\ \alpha_2[n], & n = \theta + D_1 + 1, \dots, \theta + D_2 \\ \alpha_3, & n = \theta + D_2, \dots \end{cases}$   $\alpha_1 \ge \alpha_2[\theta + D_1 + 1] \ge \dots \ge \alpha_2[\theta + D_2] = \alpha_2$ 



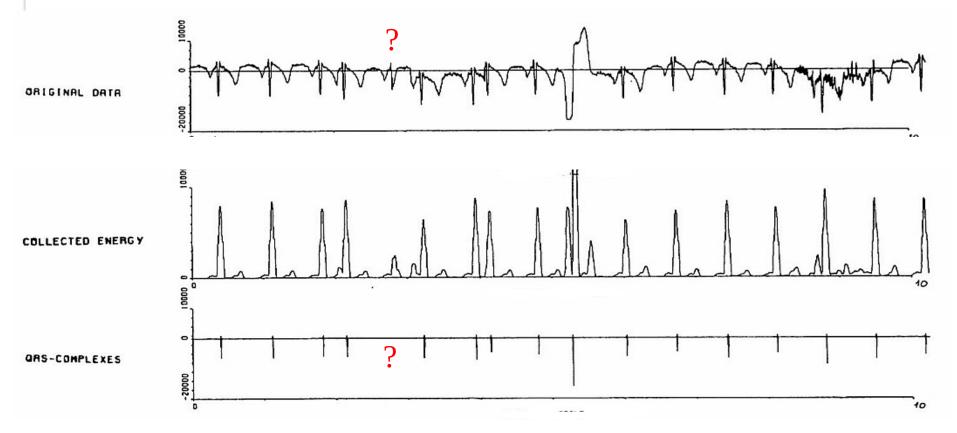


• What is Fiducial Point (FP), or reference point? (usually peak of the detection function)





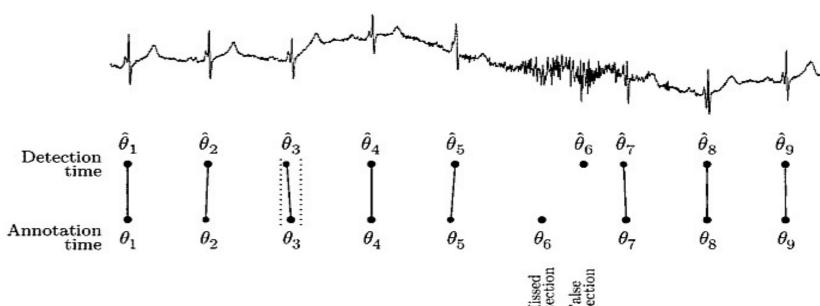
• Original ECG signal, detection function and detected QRS complexes





#### Example

- True detection of an event
- Missed detection of an event
- False detection of an event
- -? True rejection of a *non-event*? true negative (*tn*)
- true positive (*tp*)
- false negative (fn)
- false positive (*fp*)



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Performance evaluation

Classic event oriented performance matrix

		Analyzer	Analyzer
		EVENT	NON-EVENT
Reference	event	TP	FN
Reference	non-event	FP	(TN)

- TP number of correctly detected events
- FN number of missed events
- *FP* number of falsely detected events
- TN number of correctly rejected non-events
  (undefined for detection task !)



#### Performance evaluation

		Analyzer	Analyzer
		EVENT	NON-EVENT
Reference	event	TP	FN
Reference	non-event	FP	( <i>TN</i> )

#### Sensitivity:

$$Se = \frac{TP}{TP + FN}$$

The proportion of events which were detected

#### Positive predictivity:

$$+P = \frac{TP}{TP + FP}$$

The proportion of detections which actually were events

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#### Performance evaluation

		Analyzer	Analyzer
		EVENT	NON-EVENT
Reference	event	TP	FN
Reference	non-event	FP	(TN)

#### Sensitivity:

$$Se = \frac{TP}{TP + FN} \approx p (EVENT | event)$$
 An estimate of the likelihood of detecting an event

#### Positive predictivity:

$$+P = \frac{TP}{TP + FP} \approx p \text{ (event | EVENT)} \quad \text{An estimate of the likelihood} \\ \text{that a detection is an event}$$

• Approaches based on signal derivatives and digital filters (Pangerc Urška) (MIT BIH arrhythmia DB)

Se  $\approx$  99.90% +P  $\approx$  99.92%

 QRS detection based on matched filters (Haar-like filters) (Ding J J) (MIT BIH arrhythmia DB)
 Se ≈ 99,93% +P ≈ 99,88%

Silva I, Moody B, Behar J, Johnson A, Oster J, Clifford G D ,and Moody G B, Editorial: Robust detection of heart beat s in multimodal data, Physiological Measurement, Vol 36, pp. 1629-44, 2015

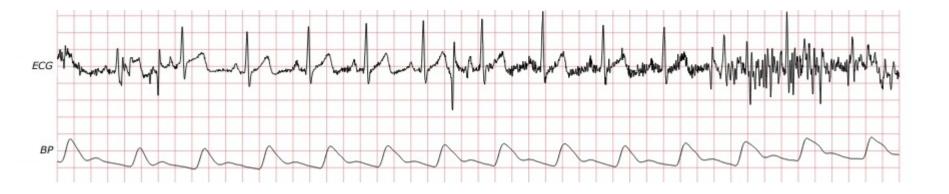
Pangerc U, and Jager F, Robust detection of heart beats in multimodal records using slope- and peak-sensitive band-pass filters, Physiological Measurement, Vol 36, pp. 1645-64, 2015

Ding J J, Huang C W, Ho Y L, Hung C S, Lin Y H, and Chen Y H, An efficient selection, scoring, and variation ratio test algorithm for ECG R-wave peak detection, Experimental & Clinical Cardiology Journal, Vol 20, pp. 4256–63, 2014

Elgendi, M, Eskofier B, Dokos S, and Abbot D, Revisiting QRS Detection Methodologies for Portable Wearable, Battery-Operated, and Wireless ECG Systems, PLoS One, Vol 9, e84018, 2014

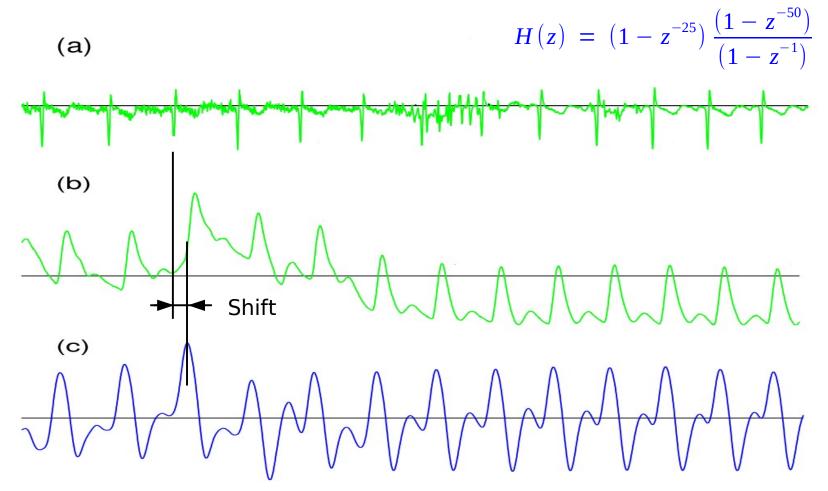
# Heart beat detection in multimodal data

- Exercises 1.f 1.g: Heart beat detection using ECG and pulsatile signals
- Use ECG signal and one of the pulsatile signals like: BP, ABP, PAP, PLETH



## Heart beat detection in multimodal data

#### • a) ECG, b) BP, c) BP filtered by slope sensitive filter:



# (Challenges in ECG signal processing today)

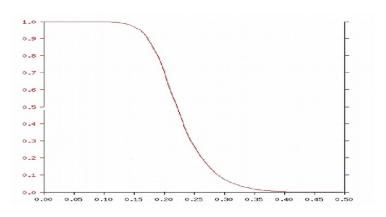
- Robust heart heat detection
- Signal quality estimation
- Reliable P wave identification
- Reliable QT interval estimation
- Distinguishing ischaemic from non-ischaemic ST changes
- Reliable heart beat classification
- Reliable rhythm analysis
- (Robust, reliable in-band signal filtering or source separation)
- (Identification of lead position misplacements or sensor shifts)
- (ECG modeling and parameter fitting)
- (The mapping of diagnostic ECG parameters to disease classifications or predictive metrics)
- (Global context pattern analysis)

• Digital Butterworth filters have a smooth frequency response and are computationally non-intensive (linear time-invariant filtering)

• Low-pass

$$|H_{L}(\Omega)|^{2} = \frac{1}{1 + \left(\frac{\Omega}{\Omega_{C}}\right)^{2N}}$$

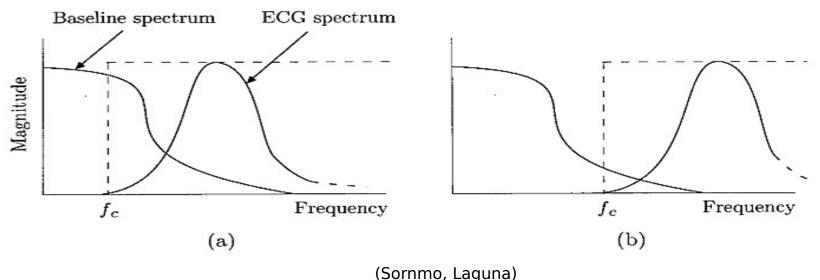
 $|H_I(\boldsymbol{\Omega})|$ 



- (High-pass)  $|H_H(\Omega)|^2 = \frac{1}{1 + \left(\frac{\Omega_C}{\Omega}\right)^{2N}}$
- Their major drawback, the phase-shifting, is especially troublesome when using high-pass filtering (will discuss Butterworth high-pass filter for EMG analysis)

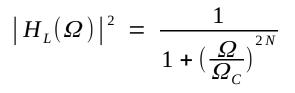


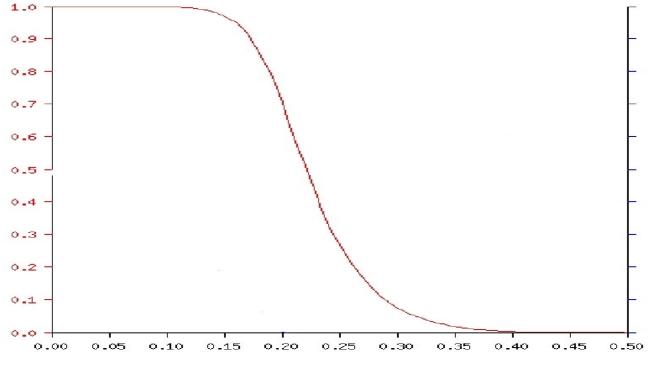
- Linear time-variant filtering (heart rate dependent filtering)
- Cut-off frequency  $f_c(n)$  is inversely proportional to the instantaneous RR interval estimate RR(n),  $f_c(n) \sim 1 / RR(n)$
- The time-varying cut-off frequency *fc(n)* is used to design a high-pass filter *h(k,n)* at every time instant *n*, where *k* denotes discrete time within the impulse response.
  - (a) low heart rate, (b) high heart rate



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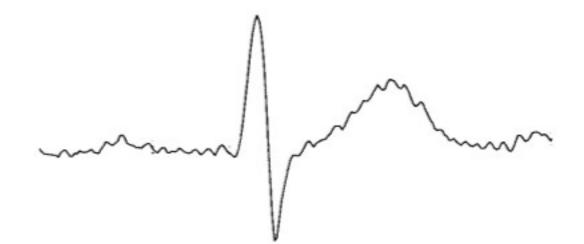
 Butterworth low-pass filtering N = 2, Fs = 200 smp/sec
 Cut-off (-3dB) at 40 Hz





# (ECG filtering, power line interference)

• Power line interference (50/60 Hz)



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# (ECG filtering, power line interference)

• Power line interference (50/60 Hz) (two zeros, two poles to make stop-band narrower)

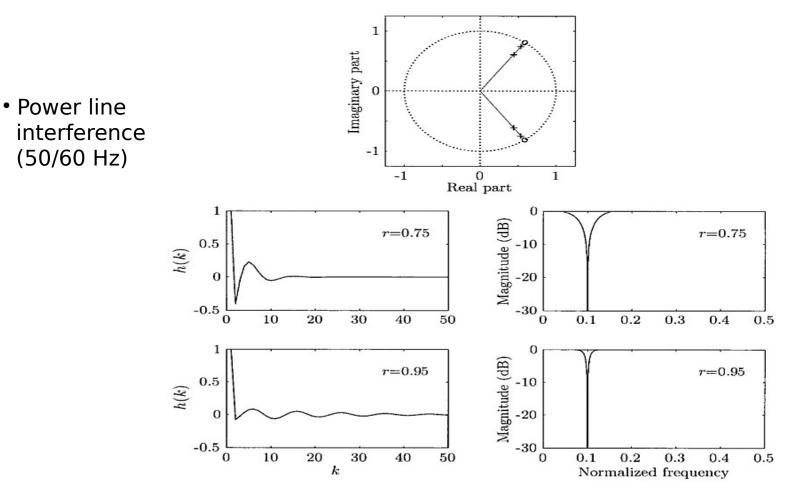
$$z_{1,2} = e^{\pm j \omega_0}$$

$$H(z) = (1 - z_1 z^{-1})(1 - z_2 z^{-1})$$
  
= 1 - 2 cos(\omega\_0) z^{-1} + z^{-2}

$$p_{1,2} = r e^{\pm \jmath \omega_0}$$

$$H(z) = \frac{(1 - z_1 z^{-1})(1 - z_2 z^{-1})}{(1 - p_1 z^{-1})(1 - p_2 z^{-1})}$$
$$= \frac{1 - 2\cos(\omega_0)z^{-1} + z^{-2}}{1 - 2r\cos(\omega_0)z^{-1} + r^2 z^{-2}}$$

# (ECG filtering, power line interference)

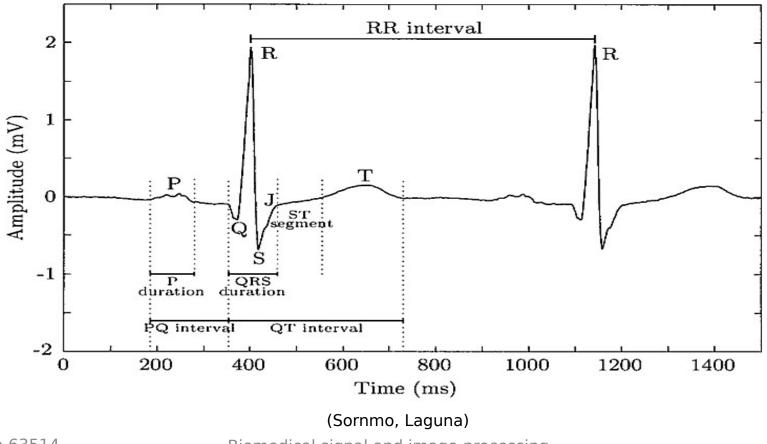


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# (Wave delineation)

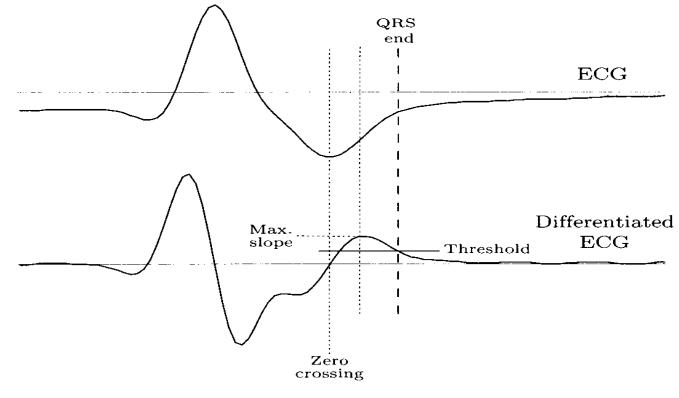
• P wave onset and offset, QRS complex onset and offset (J point), T wave onset and offset, PQ interval, QT interval





# (Wave delineation)

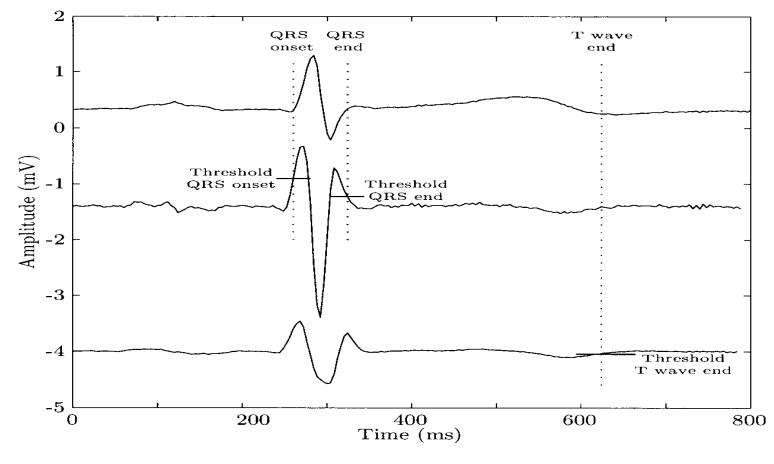
• Determining the position of QRS offset (end) (J point), the Threshold is expressed as a percentage of Maximum slope found





### (Wave delineation)

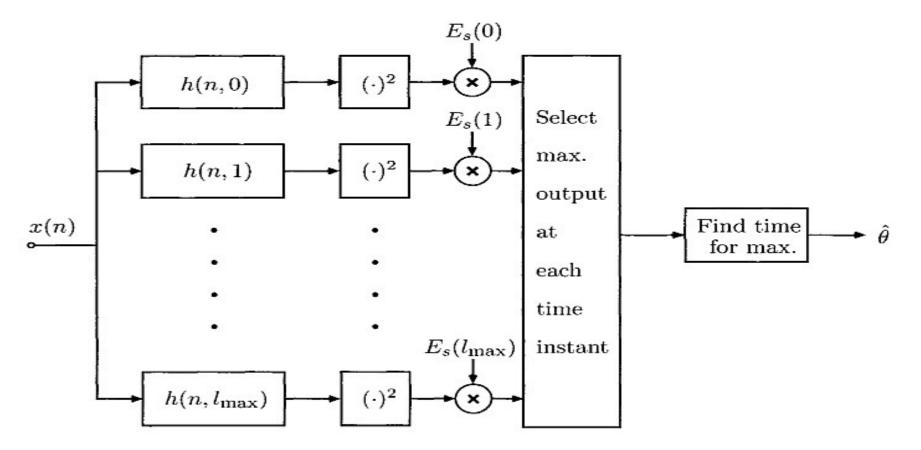
• Determining the position of QRS onset, QRS offset and T wave end



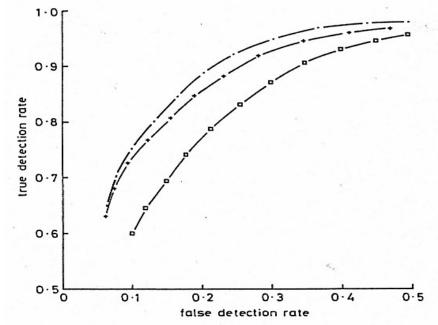
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# (Sophisticated QRS complex detection)

• Block diagram of a sophisticated QRS complex detector



- Evaluation of three different QRS complex detectors (each symbol corresponds to a certain value of the detection threshold)
- Missed detections False Negatives (*FN*), False detections False Positives (*FP*) True detection rate (*Se*) Sensitivity (*Se*), Se = TP / (TP + FN)False detection rate (1 - +P) Positive predictivity (+P), +P = TP / (TP + FP)
- Correct detections: True positives (*TP*)
- Correct rejections?
   True Negatives (TN) are undefined for the detection task !



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